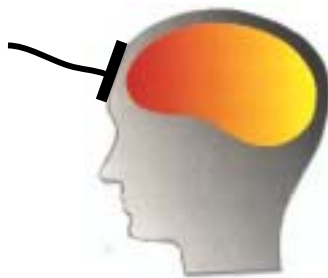


**TOS-96 Brain Oximeter**  
**TOSTEC CO., LTD**



**This purpose of this Web site is to provide an overview of the TOS-96 Brain Oximeter**

**Click “Bookmark” at the left of the screen will cause display the Table of Contents.  
Click on an item in the Table of Contents to display that item.**

**When return to TOP page, click  at left upper side on Explorer.**

**TOSTEC CO., LTD.**

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<http://www.tostec.jp>



# TOS-96

Dual Channel, Non-invasive Microvascular  
Cerebral Oxygen Saturation Monitor

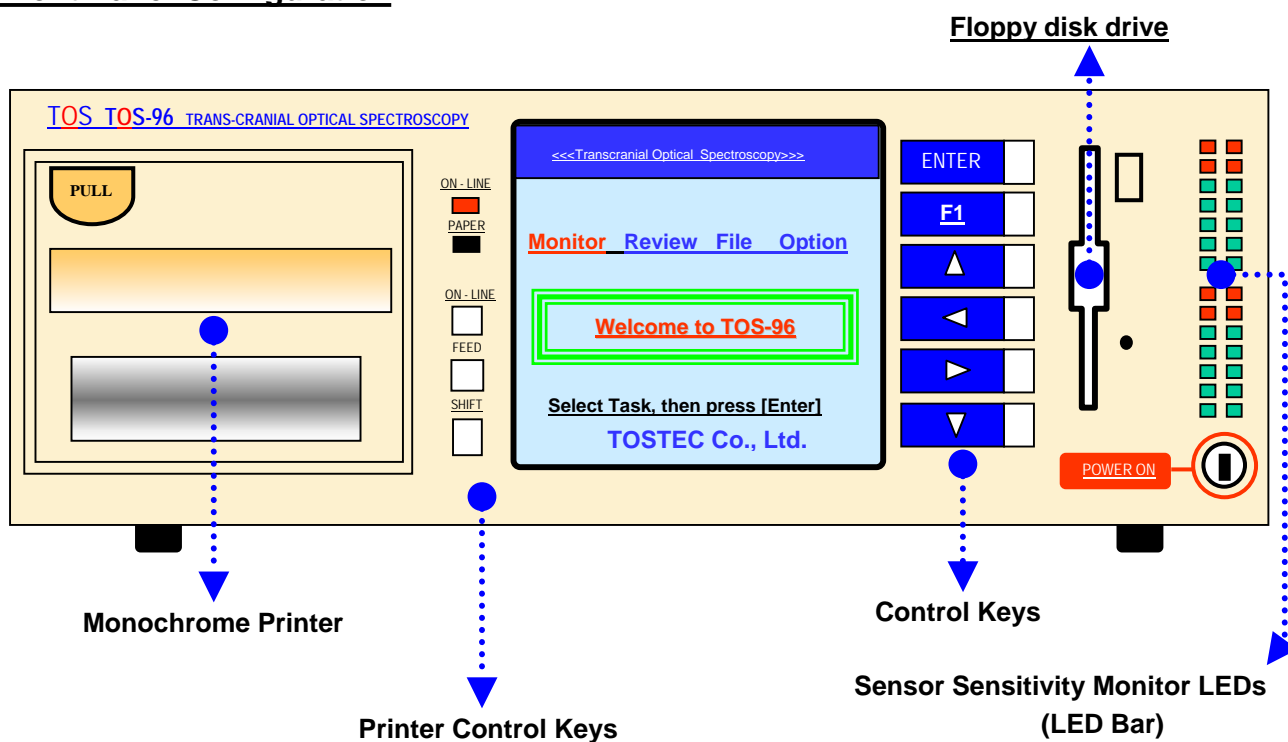
*Near Infrared is watching  
a cerebral oxygen condition.*

- Dual Channel capabilities enables simultaneous monitoring of both hemispheres.
- Cerebral blood volume index of the brain tissue underneath the sensor is measurable and displayed in real time.
- Built-in computer with 1.44MB disc drive and 420MB hard disc enables data analysis.
- Integral printer for data print out is installed.
- Re-usable sensor is guaranteed for 750 hours of continuous use.
- Sensor calibration unit is attached.



**TOSTEC** Tokyo, Japan

## TOS96 Front Panel Configuration



### Description of TOS-96 Front-Panel Components

#### Printer :

Monochrome thermal transfer printer that prints monitoring information on- and off-line.  
\* chart speeds : 3cm/10 min.

#### ON-LINE lamp :

Lit when the internal printer is set to on-line printing.

#### PAPER :

When lit, indicates that the printer paper should be replaced.

#### ON-LINE :

Used to turn on-line printing on and off.

#### FEED :

Used to feed the printer

#### SHIFT :

Unused on the current model.

#### Color monitor :

Displays monitoring information.

#### Enter :

Used to execute the selected function.

#### F1 :

Used to enter a Yes response.

#### △, ◀, ▶ and ▽ :

Move the red window used to select function and numerical values.

#### Esc :

Used to stop the execution of a function.

#### FD Drive unit :

Uses windows (DOS-V)-formatted 3.5-inch, 1.44MB floppy disks.

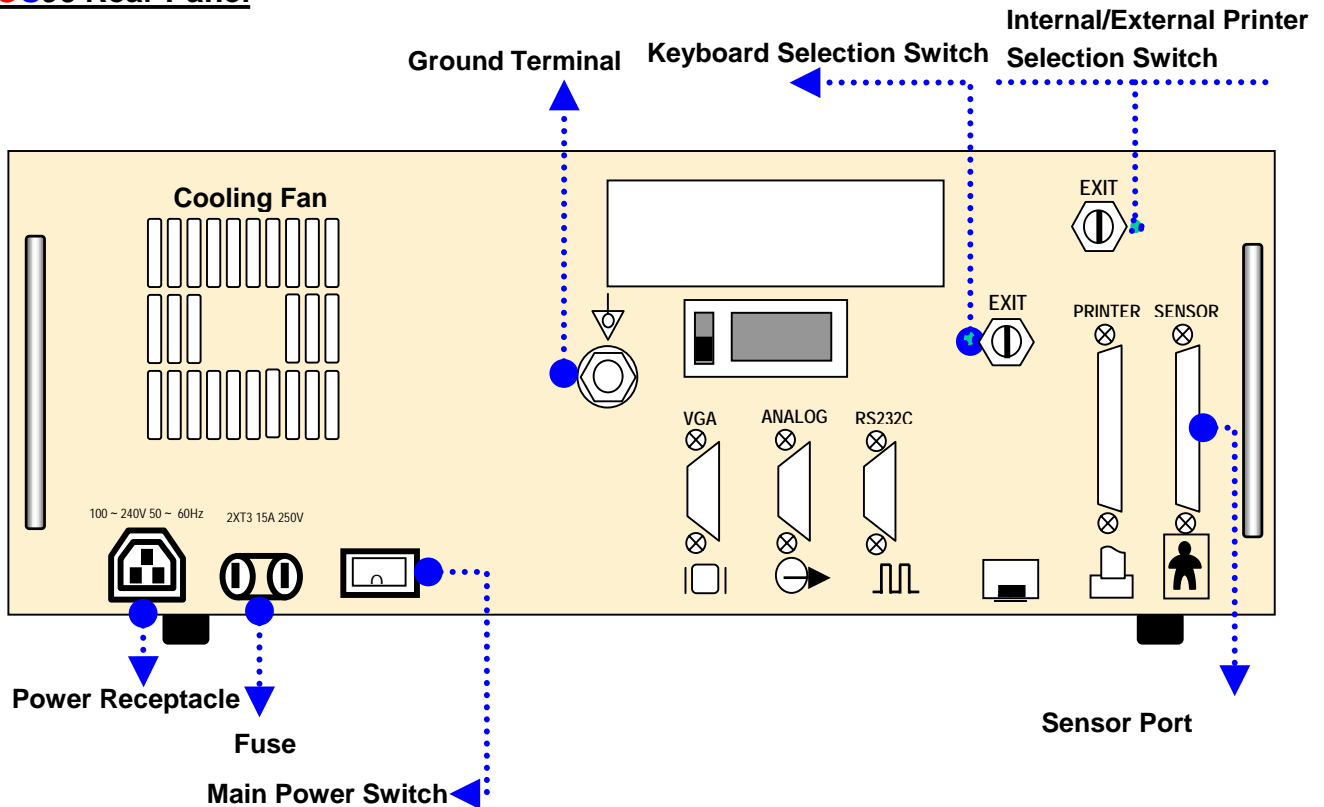
#### Sensor sensitivity monitor LEDs (LED bar):

Indicate the operating status of the sensors and the monitor status.

#### Power :

Used to turn power to the unit on and off.

## TOS96 Rear Panel



### Description of TOS-96 Front Panel Components :

1 : Cooling fan :

2-1 : Power receptacle : The includes power cable connected here.  
Connects to the nearest electrical outlet for medical devices.

2-2 : Fuse : Please do not replace the fuse. Doing so may dangerous.

2-3 : Main power switch : Press "O" to turn the unit on and "I" to turn it off.

3 : Ground terminal : Connect to the nearest ground point.

4 : VGA Port : For connecting an external monitor.

5 : Analog out port : 0-10V/0-100%.

6 : RS232C output port : Port for digital output.

7 : Hour meter (usage timer) : Total the number of hours that power to the unit has been turned on.

8 : Keyboard port : Please do not use without instructions from TOSTEC.

9 : Printer port : For connecting an ESC-type printer.

10 : Sensor cable connector port : For connecting external the included sensor cable and other side port  
should be connected to the sensor amplifier box.

11 : Printer selection switch : Used when an external printer is used.

12 : Keyboard selection switch : Please set slot se to the vertical position when monitoring is performed.

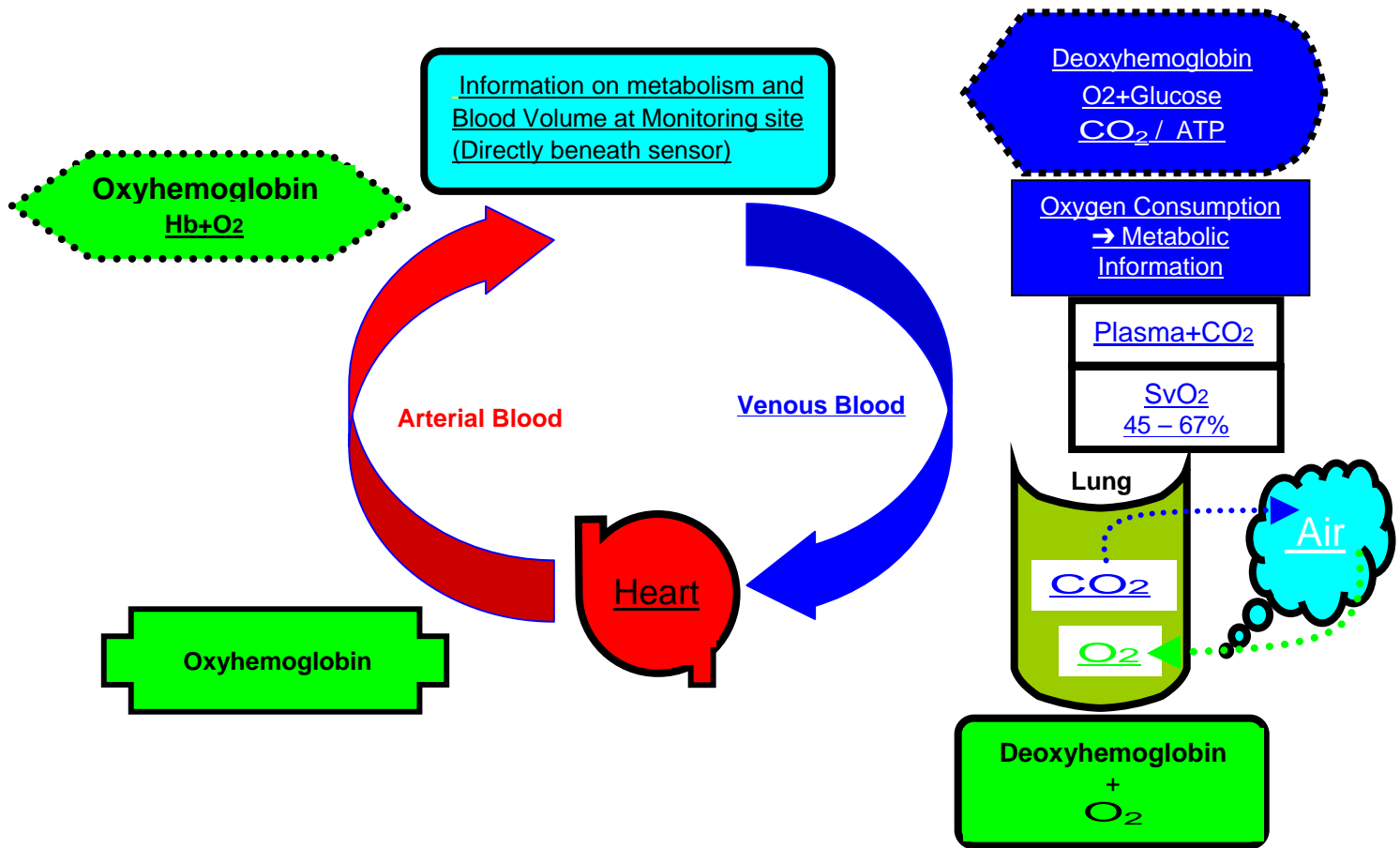
# Non-invasive Direct and Continuous BRAIN OXIMETER **TOS96**

Non-invasive monitoring of Oxygen Saturation in the Brain and muscles : **TOS96**  
**rSO<sub>2</sub>**: rSO<sub>2</sub> (regional oxygen saturation) represents the balance between the oxygen supply to the capillaries directly beneath the sensor (monitoring site) and oxygen consumption at that site. In other words, it provides information on metabolism at the monitoring site.

$$\text{Estimated } rSO_2 = ( 0.25 \times SaO_2 ) + ( 0.75 \times SvO_2 )$$

Substituting the range of normal values for SaO<sub>2</sub> (95-100%) and SvO<sub>2</sub> (45-67%) in this equation results in an rSO<sub>2</sub> values of between 57% and 75%.

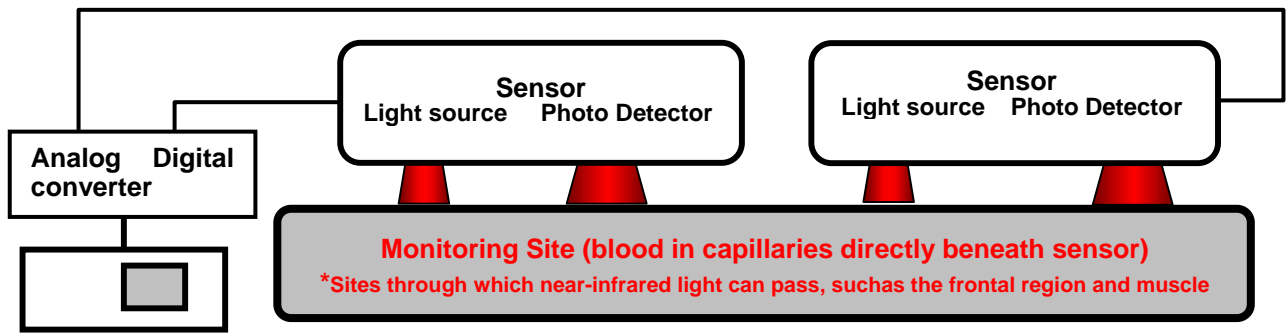
Hbl represents the percentage change in blood volume at the monitoring site ( this is not an absolute value)



Real-time monitoring of rSO<sub>2</sub> (Oxygen saturation)  
 Real-time monitoring of Hbl (percentage change in blood concentration).  
 Information on left-right differences.  
 Information on percentage change in oxyhemoglobin level  
 Information on percentage change in deoxyhemoglobin level

- All in one system
- Dual-channel monitor
- Easy to operate
- Reusable sensor
- Long-term (24hr or longer), continuous monitoring
- LED bar for monitoring sensor operating status
- Sensor for adults, children, and muscle

# BRAIN OXIMETER TOS96

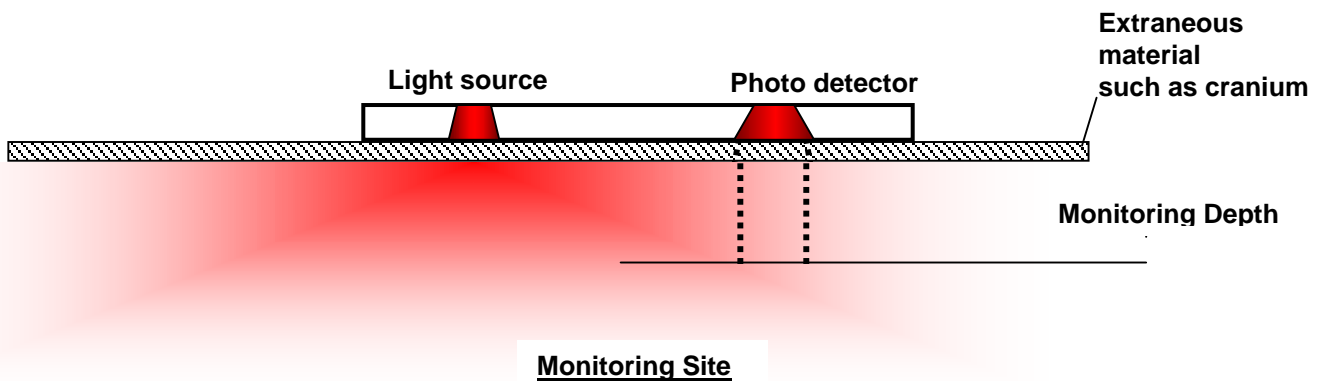


## Non-Invasive Monitoring of Oxygen Saturation in the Brain and Muscles : TOS96

### Measurement Principles of the TOS-96 Brain Oximeter

Near-infrared light at frequencies of 760nm and 850nm, which reacts specifically with deoxyhemoglobin and oxyhemoglobin, is projected onto the monitoring site from the LED light-source component of the sensor, which is attached over the monitoring site. The near-infrared light reacts with the deoxyhemoglobin and oxyhemoglobin at the site. With the light –source LED at its center, the near-infrared light propagates through the monitoring by continuous diffusion and dispersion.

As indicated in the schematic below, the energy of the near-infrared light that reacts with the - deoxyhemoglobin and oxyhemoglobin decreases as its distance from the light source increases. The near-infrared light signal (absorbance) detected by the photo detector component is converted from analog to digital and processed by the processor in the main unit.



### Calculating rSO<sub>2</sub> (regional oxygen saturation, i.e., in capillaries directly beneath sensor)

The absorbance values at 760nm and 850nm reflect the concentration of **deoxyhemoglobin** and **oxyhemoglobin**, respectively (chromophores: luminophores)

The values for **deoxyhemoglobin** and **oxyhemoglobin** are calculated based on the absorbance detected by photo detector component of the sensor.

The monitoring depth is determined by the distance between the light source and the photo detector. However, the greater this distance, the weaker the energy of the near-infrared light becomes, preventing its detection by the photo detector. With a separation of 40mm between the light source and photo detector, the monitoring depth is approximately 30mm. Since this depth corresponds to the location of cerebral cortex, it is favorable for monitoring.

Because extraneous material such as skull and muscle -- ,material other than the hemoglobin to be measured – lies between the sensor and the monitoring site, the signal that arrive at the photo detector includes information on this extraneous material. However, because oxygen saturation is calculated as an estimated  $\frac{\text{oxyhemoglobin}}{\text{deoxyhemoglobin} + \text{oxyhemoglobin}}$ , the effects of the extraneous material are eliminated by the relationship between the numerator and denominator.

$$rSO_2 = \frac{\text{OxyHb} + \text{Extraneous matters}}{\text{OxyHb} + \text{Extraneous matters} + \text{DeOxyHb} + \text{Extraneous matters}}$$

$$= \frac{\text{OxyHb}}{\text{DeOxyHb} + \text{OxyHb}}$$

**Description of Hbl : another type of data provided by th TOS-96**

Developed by TOSTEC, Hbl (hemoglobin index) is a numerical value that indicates blood concentration. Hbl is calculated using the total deoxyhemoglobin and oxyhemoglobin obtained at the start of monitoring, as the base value, or b (oxyhemoglobin b + deoxyhemoglobin b). Supposing, for example, that the value at the start of monitoring, n (oxyhemoglobin n + deoxyhemoglobin n), was 5 and value at an arbitrary time point (oxyhemoglobin n + deoxyhemoglobin n) was 4.9, Hbl for that time point would be 4.9/5, or 0.98. If the value at the arbitrary time point was 5.1, Hbl would be 5.1/5, or 1.02. Because extraneous material would affect both the numerator and denominator, its effects would be cancelled out. Thus, Hbl is hemoglobin information that is unaffected by such material. However, because Hbl represents the percentage change as compared with the baseline value at start of monitoring, which is a relative value, it cannot be used to compare individual subjects or to establish a range of normal value. For all subject, monitoring normally starts with Hbl at or near 1.

$$Hbl = \frac{\text{OxyHb}_n + \text{Extraneous matters} + \text{DeOxyHb}_n + \text{Extraneous matters}}{\text{OxyHb}_b + \text{Extraneous matters} + \text{DeOxyHb}_b + \text{Extraneous matters}}$$

$$= \frac{\text{OxyHb}_n + \text{DeOxyHb}_n}{\text{OxyHb}_b + \text{DeOxyHb}_b}$$

———> Value at arbitrary time point after the start of monitoring  
 ———> Value at the start of monitoring

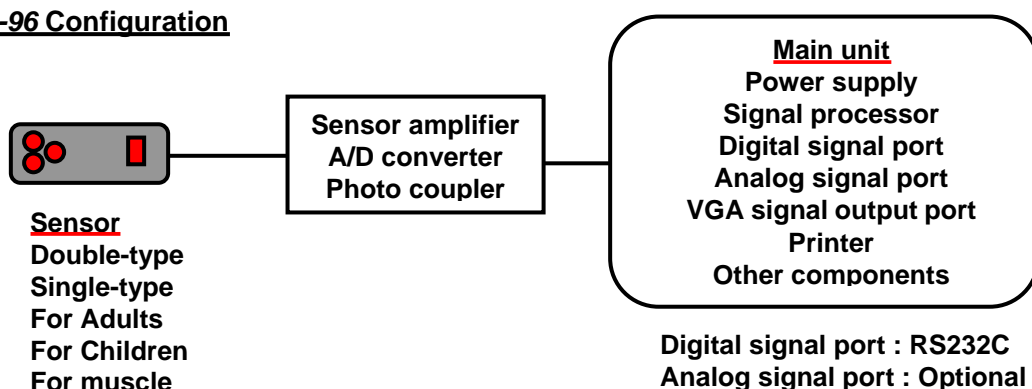
An increase in Hbl reflects an increase in total oxyhemoglobin and deoxyhemoglobin at the monitoring site as compared with the start of monitoring, while a decrease in Hbl means that total oxyhemoglobin and deoxyhemoglobin at the monitoring site decrease.

**Note!!**

Hbl indicates the percentage change, a relative value. Therefore, it cannot be used for purposes such as determining a range of normal values or comparing individual patients.

TOSTEC is currently developing an index that will permit the normal range to be determined.

**TOS-96 Configuration**



## Data Provided by the **TOS96** Brain Oximeter :

### **rSO<sub>2</sub>** :

rSO<sub>2</sub> (regional oxygen saturation) represents the balance between the oxygen supply to the capillaries directly beneath the sensor (monitoring site) and oxygen consumption at that site. In other words, it provides data on metabolism at the monitoring site.

The monitoring depth depends on the form of sensor used. With a sensor for adults, the monitoring depth is approximately 30mm. The information obtained is expressed as a digital number (%), updated every second) and as a trend graph (updated every 5 seconds). The blood at the monitoring site is in the capillaries and is therefore a mixture of arterial and venous blood. Consequently, oxygen saturation at the monitoring site can be estimated by the formula  $(0.25 \times SaO_2) + (0.75 \times SvO_2)$ . Assuming that the **normal range for SaO<sub>2</sub>** is 95% to 100% and that for SvO<sub>2</sub> is 45% to 67%, the normal range for rSO<sub>2</sub> can be estimated to be 57% to 75%.

### **Example of rSO<sub>2</sub> Application :**

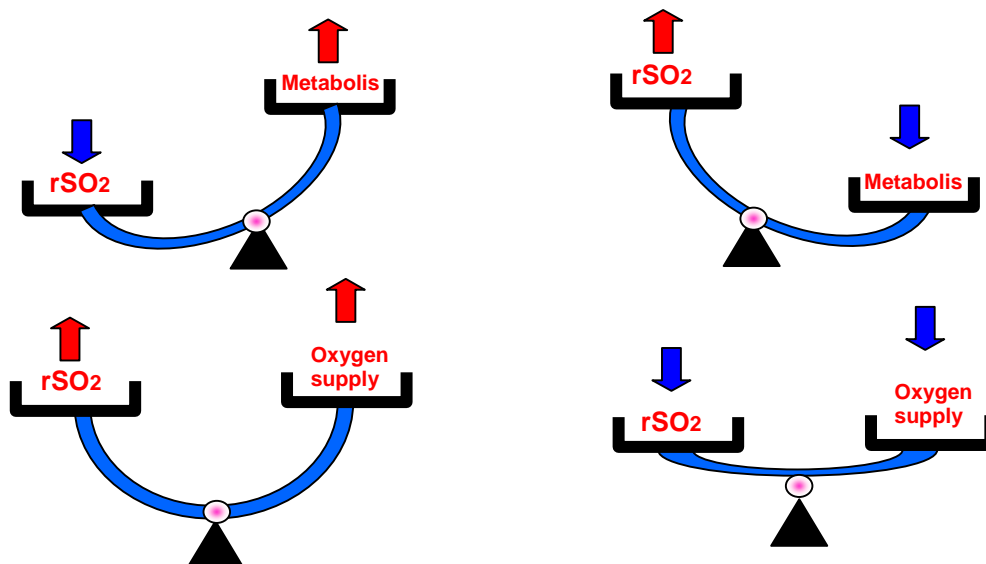
If there has been **no change in the oxygen supply or blood volume at the monitoring site**, an **increase in rSO<sub>2</sub>** would indicate that oxygen consumption at the monitoring site **decrease**, while a **decrease in rSO<sub>2</sub>** would indicate that **oxygen consumption increased**.

If there has been **no change in the oxygen consumption (metabolism) at the monitoring site**, and **increase in rSO<sub>2</sub>** would indicate that the oxygen supply to **the monitoring site increase**, while a **decrease in rSO<sub>2</sub>** would indicate that the **oxygen supply decreased**.

Caution should be exercised in identifying the cause of a change in rSO<sub>2</sub> if **the oxygen/blood supply changes simultaneously with oxygen demand at the monitoring site**.

There appear to be many cases in which the direct cause of the change is related to cardiac function or the vascular system that supplies blood to the monitoring site. rSO<sub>2</sub> changes with blood pressure, pulse rate, stroke volume or the occurrence or elimination of vascular stenosis or occlusion that affects the monitoring site. In other words, it is necessary to determine whether the change in rSO<sub>2</sub> is due to a change at the monitoring site, a change in the functions that supply oxygen to the monitoring site, or a combination of these factors.

	rSO <sub>2</sub>	Oxygen consumption	Oxygen supply
No change in oxygen supply or blood volume monitoring site	↑	↓	→
	↓	↑	→
No change in oxygen consumption (metabolism) at monitoring site	↑	→	↑
	↓	→	↓
Change in oxygen/blood supply to monitoring site with simultaneous change in oxygen demand at site	↑	↑ ↓ →	↑ ↓ →
	↓	↑ ↓ →	↑ ↓ →



If information on blood volume at the monitoring site (**deoxyhemoglobin + oxyhemoglobin**) is available, more accurate information on the **oxygen supply** and **consumption at the monitoring site** can be obtained.

If **oxyhemoglobin increases**, it can be inferred that either the oxygen supply to the monitoring site increased or oxygen demand at the site decreased.

A **decrease in oxyhemoglobin** indicates that either the oxygen supply to the monitoring site decreased or oxygen demand increased.

If **deoxyhemoglobin increases**, it can be inferred that either more carbon dioxide was delivered to monitoring site or oxygen consumption at the monitoring site increased, resulting in an increase in the amount of carbon dioxide released.

A **decrease in deoxyhemoglobin** indicates that either less carbon dioxide was delivered to the monitoring site or oxygen consumption at the monitoring site decreased, resulting in a decrease in the amount of carbon dioxide released.

The total **oxyhemoglobin** and **deoxyhemoglobin** provides data on the overall blood volume at the monitoring site. This value, **Hbl**, is described in the next section.

### **Hbl :**

This index, which indicates the total **oxyhemoglobin** and **deoxyhemoglobin** at the monitoring site, is displayed as a digital number and trend graph.

As was explained in the previous section, Hbl is unaffected by extraneous material such as the patient's cranium and provides data on hemoglobin only.

Because Hbl is a relative value, the Hbl levels of individual patients cannot be compared, and no normal range for Hbl can be established. For all patients, monitoring starts with Hbl at or near 1.

**An increase in Hbl means that the blood volume at the monitoring site increased as compared with the start of monitoring, while a decrease in Hbl indicates that the blood volume decreased.**

### **Oxyhemoglobin**

The percentage change in oxyhemoglobin is displayed in a trend graph. Because it is expressed as a relative value, the oxyhemoglobin value cannot be used to establish a normal range or compare individual patients. An increase in the value indicates that the oxyhemoglobin concentration at the monitoring site increased as compared with the start of monitoring, while a decrease in the value means that the concentration decreased.

### **Deoxyhemoglobin**

The percentage change in **deoxyhemoglobin** is displayed in a trend graph. Because it is expressed as a relative value, the deoxyhemoglobin value cannot be used to establish a normal range or compare individual patients. An increase in the value indicates that the deoxyhemoglobin concentration at the monitoring site increased as compared with the start of monitoring, while a decrease in the value means that the concentration decreased.

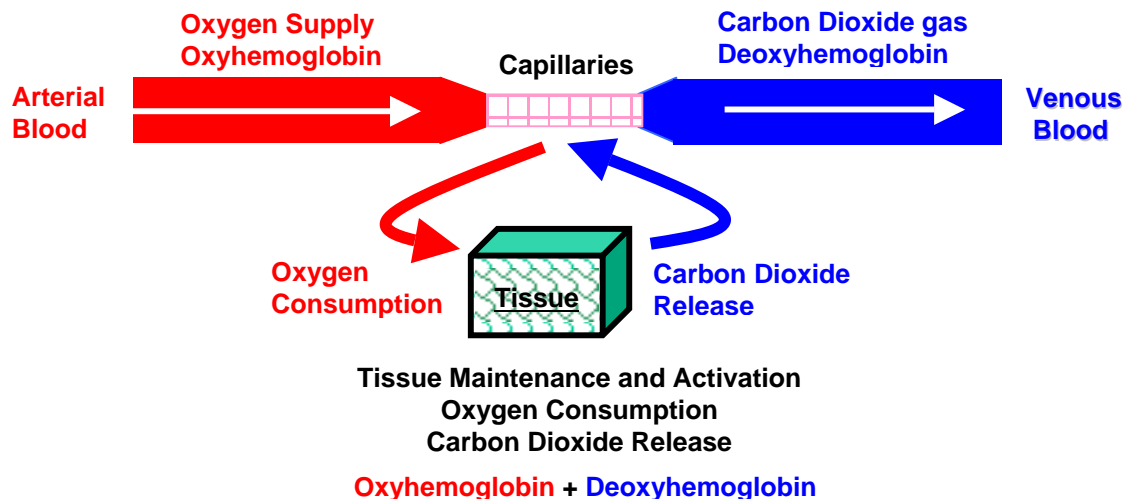
Deoxyhemoglobin can be a product of the patient's metabolism, or it can be produced according to the gas exchange rate. If the patient's gas exchange rate can be assumed to be constant, their metabolic state can be directly inferred from the **deoxyhemoglobin** value.

### **Left-Right Difference**

Values obtained by subtracting the oxygen saturation obtained with the right sensor from that obtained with the left sensor (left sensor signal – right sensor signal) are displayed in a trend graph. These values can be used to compare a control site with the affected area. With ASA, placing one sensor over a normal site and the other over the affected area allows the condition of the affected area to be observed.

## Summary of Data Provided by the TOS-96

The data provided by the TOS-96 are described in the following figure.



Arterial blood with an oxygen saturation level of approximately 100% is supplied

In general, metabolism occurs in tissues for tissue maintenance, and during this process oxygen is consumed and carbon dioxide produced. During normal metabolism, the level of oxygen consumption is constant, and the level of carbon dioxide produced is also constant. If the level of tissue activation increases, metabolism is enhanced, and more oxygen is consumed and more carbon dioxide produced than during normal metabolism. A decrease in the level of tissue activation results in a decrease in metabolism, with less oxygen consumed and less carbon dioxide produced than during normal metabolism.

During normal metabolism, the levels of oxygen consumed and carbon dioxide produced are constant. Therefore,  $rSO_2$  remains at a constant level in the normal range. However, it should be noted that  $rSO_2$  also may remain unchanged if an increase in oxygen demand by the tissues is met by a sufficient change in the oxygen supply. With increased tissue activation, metabolism is enhanced, and more oxygen is consumed and more carbon dioxide produced than during normal metabolism. Consequently,  $rSO_2$  will decrease. It also will decrease if the oxygen supply to the tissue decreases.

There may be reservations about using  $rSO_2$  as the only information for determining whether a decrease in  $rSO_2$  is due to enhanced metabolism in the tissue or to decreased oxygen supply to the tissue. In this case, taking Hbl, oxyhemoglobin, and deoxyhemoglobin into account allows a more accurate determination.

A decrease in the level of tissue activation results in a decrease in metabolism, with less oxygen consumed and less carbon dioxide produced than during normal metabolism.

Consequently,  $rSO_2$  will increase. Here again, more accurate determination of the cause of the increase may be possible by taking Hbl, oxyhemoglobin, and deoxyhemoglobin into account.

## **Hardware Features**

### **All-in-one system :**

Internal color monitor, black-and-white printer, hard disk, and floppy disk drive

### **2-channel monitor :**

Uses sensors for the left and right sides.

### **Reusable sensors :**

Sensors can be used repeatedly. A sensor can be used continuously for at least 750 hr.

### **Sensors can be sterilized with EO gas (non-thermal, non-liquid sterilization) :**

Sensors can be sterilized with ethylene oxide gas or formalin. Sensor surface can be wiped with alcohol gauze.

### **Allows continuous monitoring for 24 hr or longer :**

The energy of the LEDs used in the system is infinitesimal and unlikely to produce red spots or other skin damage.

### **Sensor operating status monitor :**

Constantly monitors the operating status of the sensors and the status of the monitor signal.

### **Sensors :**

Single- and double-type sensors (left-right pair) are available, with versions of each type for adults, children, and muscle monitoring.

## Specifications

<b>Data Provided</b>	<b>The following types of data are provided on- and off-line</b> rSO <sub>2</sub> : trend graph and numerical values Hbl (hemoglobin index): trend graph and numerical values Information on left-right difference: trend graph Oxyhemoglobin and deoxyhemoglobin: trend graph
<b>Accuracy</b>	rSO <sub>2</sub> : 100 ~ 80%    ± 5% 80 ~ 40%        ± 3% 40 ~ 0%         ± 5%
<b>Data recording medium</b>	Internal hard disk: > 1 GB (holds at least 3 years' worth of data) Floppy disk: 1.44 MB, 3.5-inch disk *Each floppy disk can store approximately 26 hr of data
<b>Display screen</b>	Color TFT-LCD 115.2 x 84.2 mm
<b>CPU</b>	INTEL
<b>Light source</b>	Light-emitting diode
<b>Photo detector</b>	Silicon diode
<b>Internal printer</b>	Black-and-white thermal transfer printer, chart speed : 3cm/10min
<b>Output</b>	Analog output: 0-10V *Available separately Digital output: RS232C VGA output: Printer port: ESC/P type Floppy disk drive: DOS-V, 1.44 MB, 3.5 inch
<b>Operating temperature</b>	+16 – 32
<b>Operating humidity</b>	20 – 80% non-condensing
<b>Power supply</b>	100 – 240VAC
<b>Operating power</b>	140VA
<b>Leakage current</b>	< 0.5mA
<b>Dimensions</b>	420W x 460D x 130H (cm)
<b>Weight</b>	14.5Kg
<b>Other specifications</b>	Japanese pharmaceutical license:20800BZZ00343000 and IEC-601,

\*The analog output port is available separately; please note that it is not included with the standard unit.

\*\*These specifications may be improved without prior notification

**Sensor Types and Monitoring Depth**

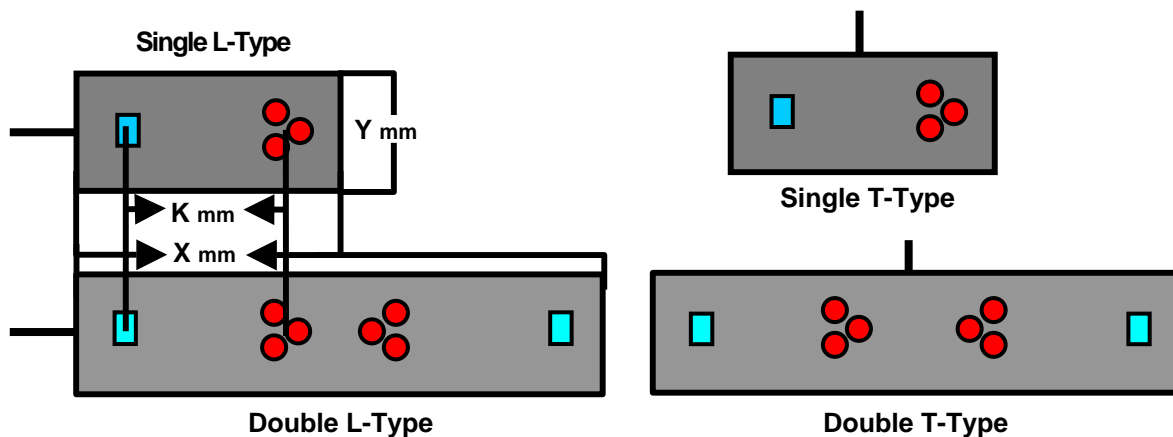
The following is a description of the TOS sensors.

Each sensor consists of 3 LEDs (light source component) and 1 silicon photodiode (photo detector component). The LEDs of the light source component project near-infrared light on the monitoring site, and the photo detector component detects near-infrared light that has reacted with oxyhemoglobin and deoxyhemoglobin and at their crossover point. The near-infrared light is projected on the monitoring site as 0.2 mSec pulses at an intensity of 12 mW/cm<sup>2</sup> and rate of 50 pulses/sec (total of 150 pulses/sec for the 3 wavelengths).

The photo detector component detects the near-infrared light that is projected from the light source component onto the monitoring site and absorption-attenuated by material such as tissue and hemoglobin. This analog signal is converted to a digital signal by the sensor amplifier box and then sent to the processor of the main unit.

A 1,500 mm sensor cable is the standard cable provided, but cables up to 3,000 mm long are available. The sensors must be stored in a clean and dry condition.

Sensors are available as either the single- or double-type, depending on their shape, and each of these types comes in either the T- or L-type, depending on where the cable attaches.



Monitoring Depth : D ± 3mm

Sensor type	D mm	K mm	X mm	Y mm
Single L for Adults	28mm	40mm	80mm	40mm
Single T for Adults	28mm	40mm	80mm	40mm
Double L for Adults	28mm	40mm	160mm	40 mm
Double T for Adults	28mm	40mm	160mm	40mm
Single L for Children	20mm	30mm	80mm	40mm
Single T for Children	20mm	30mm	80mm	40mm
Double L for Children	20mm	30mm	140mm	40mm
Double T for Children	20mm	30mm	140mm	40mm
Single T for Children	15mm	20mm	80mm	40mm
Double T for Children	15mm	20mm	120mm	40mm
For Muscle & Tissue	7mm	10mm	40mm	40mm

**Comparison with Pules oxynetry and Oxymetry Methods**

The differences between the TOS-96 Brain Oximeter, pulse oxymetry, and SjO<sub>2</sub> monitoring are shown below.

	<b>Brain Oximeter</b>	<b>Pulse Oximeter</b>	<b>SjO<sub>2</sub></b>
<b>Sensor location</b>	Sites through which near-infrared light passes: e.g., the frontal region and muscle	Tips of finger, toes	Jugular bulb
<b>Monitoring material</b>	Hb at the monitoring site	Arterial blood in tips of finger, toes	Venous blood in jugular bulb
<b>Type of information provided</b>	Oxygen saturation in capillaries at the monitoring site Change in blood volume at the monitoring site Information on left-right difference Change in oxyhemoglobin and deoxyhemoglobin levels	Oxygen saturation of arterial blood in tips of finger and toes  Pulse rate	Oxygen saturation of venous blood in jugular bulb
<b>Condition for use</b>	Can be used in subjects with hypotension and bradycardia Completely non--invasive	Blood pressure and pulse required	highly invasive
<b>Normal values</b>	55% to 75% Monitoring values determined by the balance between oxygen supply and oxygen consumption at the monitoring site.	95% to 100% Monitoring assumes the values for oxygen saturation in arterial blood of tips of fingers and toes are proportional to the pulmonary gas exchange rate.	40% to 67% Monitoring values change depending on the location of the sensor chip. Provides whole-brain information.

**Additional note:**

Transcranial Doppler ultrasound utilizes the Doppler principle to monitor blood flow velocity beneath areas through which 2 MHz ultrasound can pass. To obtain information on blood flow velocity in the head, such monitoring is performed in the area of the temple where the cranium is thin. The data are expressed in units of cm/sec. Transcranial Doppler permits completely non-invasive monitoring. This type of monitoring requires skill, and data cannot be obtained if the cranium is too thick. Moreover, the blood flow velocity varies depending on the angle at which the ultrasound crosses the blood vessel.

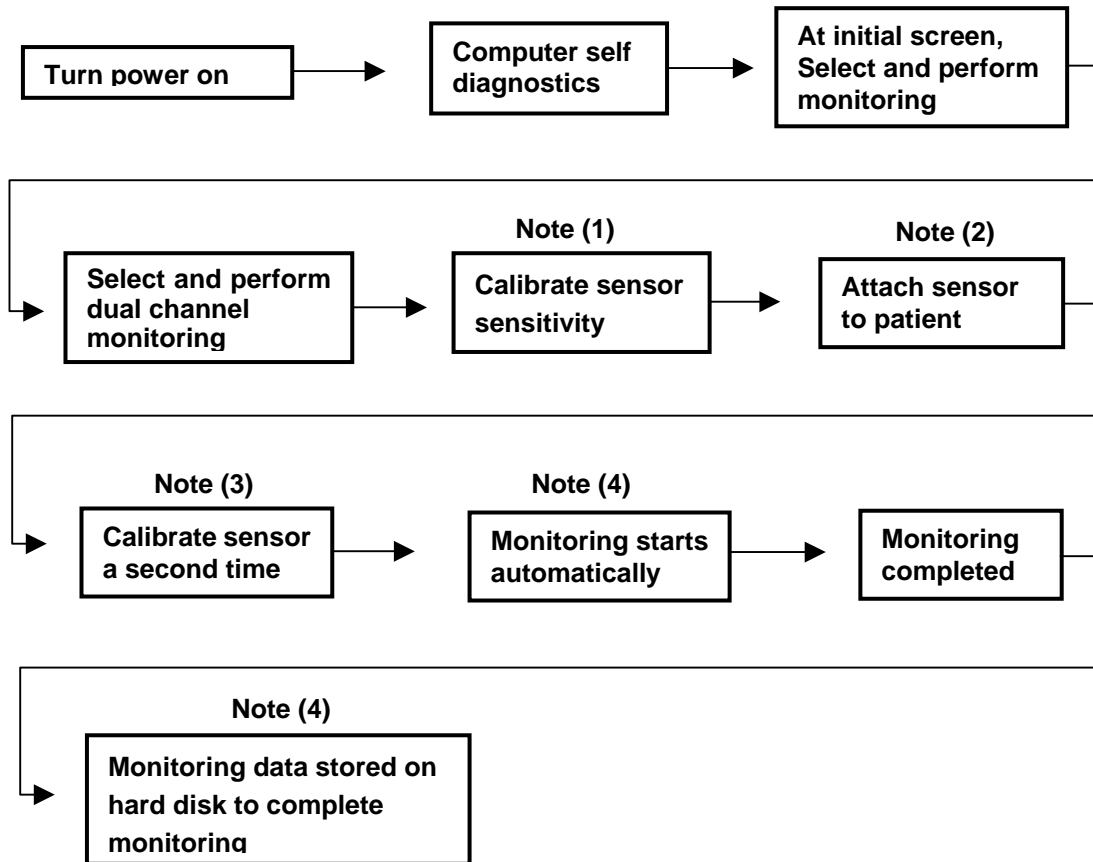
## Operating Flowchart

The following describes the flow of operations of the **TOS-96**.

The TOS-96 is operated using the 7-key keypad located on the front panel.

The following describes normal 2-channel monitoring, from start to finish.

Each screen displays the operating procedure to be carried out next.



### Note (1)

Sensitivity of light source and photo detector calibrated to the prescribed ratio.

### Note (2)

The sensor must be attached tightly to the skin so that external light does not mix with the light detected by the photo detector. The sensor is made from a flexible silicon material and therefore fits closely to the skin. To attach the sensor, first firmly apply 2-sided medical adhesive tape to the monitoring site, and place the sensor over the tape. Press down on the edges of the sensor with your fingers to prevent contamination by external light. An effective way to prevent external light from entering beneath the sensor is hold down the edges of the sensor with tape.

### Note (3)

The second sensor calibration is performed to eliminate the absorption and dispersion of the near-infrared light caused by material such as the cranium and muscle tissue, which varies from patient to patient. This calibration takes 20 seconds. When it is complete, monitoring begins automatically.

### Note (4)

The monitoring data also can be stored directly on a floppy disk.

## Clinical Applications of the TOS-96

The TOS-96 is used primarily in the fields indicated below.

It can be used to obtain sequential information on oxygen saturation, metabolism, blood, and oxyhemoglobin and deoxyhemoglobin in the capillaries of tissues directly beneath the sensor. It can therefore be used in the case of clinical symptoms for which metabolic and blood-related information for the monitoring site is needed.

The TOS-96 is used in anesthesiology, cardiac surgery, vascular surgery, thoracic surgery, pediatrics, neurosurgery, neuropsychiatry, neurological checkups, emergency medicine, operating rooms, intensive care, neurosurgical intensive care, rehabilitation, health sciences, and sports medicine. Monitoring with the TOS-96 is used for purposes including circulatory management for cerebroprotection; peripheral circulatory treatment evaluation and postoperative management; measurement evaluation of the effect of drugs and other treatments; and examination and stress testing of the cerebral and peripheral circulation.

The following is an overview of these applications by field.

### **1) Anesthesia management**

Management of cerebral circulation for cerebroprotection:

Prevention of perioperative brain damage due to factors such as position changes, neck torsion pressure, and reduced cerebral perfusion pressure

Under general anesthesia, the sympathetic reflexes are inhibited and cerebral blood volume decreases significantly due to the low position of the head. Autoregulation of cerebral blood flow is lost during anesthesia, but cerebral blood flow can be safely maintained by using the values for  $rSO_2$  and Hbl obtained immediately prior to anesthesia induction as reference levels to manage functions such as ventilation and blood pressure from the start of anesthesia until the patient awakens. With intravenous and inhaled anesthetics, the effect on cerebral blood flow varies depending on the anesthetic used. Following anesthesia induction, oxygen saturation can gradually decrease and approach hypoxia. However, by monitoring  $rSO_2$  and Hbl and controlling factors such as  $CO_2$ , blood pressure, pulse rate, and ventilation, a proper balance between oxygen supply and demand can be maintained. Inadequate management of the patient's physiological functions can cause blood pressure disturbances, and problems such as hyperventilation, ventilatory failure, and hypotension may lead to long-term hypoxia, possibly resulting in postoperative sequelae.

#### **Tips!!**

During monitoring, close attention should be paid to the percentage change in Hbl, for which a value approximately 1 is displayed at the start of monitoring. An increase in this value means that the concentration of the blood increased as compared with the start of monitoring, while a decrease indicates that the blood concentration decreased. Because Hbl indicates total deoxyhemoglobin and oxyhemoglobin, it also can be used as an approximate measure of cerebral blood volume.

In some cases,  $rSO_2$  may remain unchanged even though the oxygen supply to the monitoring site changes. This occurs if the change in the oxygen supply is in a range that is sufficient to meet oxygen demand at the monitoring site. For more rigorous observation of the change in the oxygen supply, it is recommended that the percentage change in oxyhemoglobin and deoxyhemoglobin be observed at the same time as  $rSO_2$ .

By displaying the percentage change in oxyhemoglobin and deoxyhemoglobin on the data display screen of the TOS-96 and printing  $rSO_2$  and Hbl data to the printer, these 4 types of data can be observed together.

### **2) Cardiovascular surgery**

Management of cerebral circulation for cerebroprotection:

Management and monitoring of cerebral circulation and percutaneous cardiopulmonary support (management of circulatory status with PCPS)

It is estimated that approximately 10% of patients who undergo heart surgery have postoperative brain sequelae (affecting brain function). Examples of applications of the TOS-96 include monitoring of the cerebral circulation to prevent postoperative brain dysfunction resulting from hypoperfusion in procedures such as replacement of the thoracic aorta, aortic arch, thoracic descending aorta, and ascending aorta; coronary artery bypass; revascularization; mitral, aortic, and tricuspid valve replacement; and circulatory arrest during the replacement of a thoracic aortic aneurysm with a synthetic graft. Other examples include monitoring of the cerebral circulation to prevent brain damage due to hypoperfusion during rewarming by extracorporeal circulation, to detect risk for perioperative neurological complications during selective

cerebral perfusion and prevent such complications, and to prevent neurological complications caused by bending of the graft during surgery to replace a blood vessel with a synthetic graft (even with successful revascularization, bending may occur at times such as suture removal, resulting in damage due to inadequate blood flow).

In open-heart surgery, a heart-lung machine is used, and problems may occur during cannulation or withdrawal of this support. Even during pumping, when blood should be flowing to the brain, the blood flow may actually be insufficient (hypoperfusion) due [Page 18]

to bending or pressure on the feeding vessel. Based on the rSO<sub>2</sub> and Hbl information, the pump operator, anesthesiologist, and surgeon can detect these abnormalities and safely take measures to prevent an accident.

rSO<sub>2</sub> and Hbl also can be observed using a TOS-96 sensor placed on the forehead to allow monitoring for hypoperfusion and abrupt changes in cerebral blood flow and thereby detect cases such as blockage of a cerebral blood vessel that occurs during surgery when thrombus or other material travels down the bloodstream. Although imperfect, such monitoring enables appropriate measures to be undertaken immediately in such cases.

**3) Management of cerebral circulation during pediatric heart surgery (e.g., for congenital heart or pulmonary artery malformation) and extracorporeal membrane oxygenation (ECMO) in neonates and premature infants**  
Management of cerebral and peripheral circulation and assisted circulation for cerebroprotection:

In neonates and infants, slight changes in position or torsion of the neck can impair blood flow. Because the TOS-96 sensors for infants are soft, they can be attached firmly to small heads, allowing stable, long-term monitoring of neonates, premature infants, and other infants during surgery and on the ward. In addition, the energy level of the near-infrared light is miniscule, which is also conducive to long-term monitoring.

#### **4) Neurosurgery**

Management of cerebral circulation for cerebroprotection:

Cerebral blood flow must be monitored before and after procedures such as internal carotid endarterectomy, tumorectomy, intravascular thrombolysis, CNS surgery, and the various bypass procedures. It is difficult to obtain blood-flow information about the surgical field itself due to the surface area of the TOS-96 sensor. However, in internal carotid endarterectomy, a sensor can be placed on the side of the forehead ipsilateral to the affected area, allowing the presence or absence of collaterals to be determined and postoperative circulatory improvement to be directly monitored. The TOS-96 is also effective for preventing postoperative hyperemia, hyperperfusion, and cerebral edema.

#### **5) Other surgical procedures**

Peripheral hemodynamics can be monitored by placing sensors in the region supplied by the blood vessels of interest.

To monitor ischemia of the lower extremities during surgery for severe lower-extremity ischemia, evaluation and management of peripheral circulatory dynamics following revascularization can be performed by pre-, intra-, and postoperative monitoring of the dorso-ventral muscles and the plantar region. In addition, measurement of cerebral oxygen saturation during procedures in the neck region, such as right thyroid lobectomy and venous ligation as part of a dental procedure, is effective for managing cerebral and peripheral circulation.

#### **6) Emergency medicine**

Applications such as evaluation of cerebral oxygen status on hospital arrival and management and evaluation of cerebral and peripheral blood flow during and after emergency surgery:

The TOS-96 can be used to monitor and manage peripheral circulation for the purpose of cardiopulmonary resuscitation (CPR) and cerebroprotection. Such monitoring and management includes the evaluation of cerebral and peripheral blood flow and oxygenation during CPR, management of cerebral and peripheral circulation following treatment for severe head trauma or cerebral or myocardial infarction, and preventive management of vasospasm following treatment for subarachnoid hemorrhage.

#### **7) Long-term, continuous monitoring of cerebral blood flow in the ICU**

Monitoring and evaluation of circulatory status following drug administration or other intervention and monitoring during fibrinolytic therapy:

Continuous monitoring is performed to detect hyperemia, congestion, vasospasm, and hypoxia for postoperative management in cardiac and neurological procedures to prevent brain damage during hypothermia therapy and following surgery for head trauma or severe brain injury. With cerebral hypothermia, continuous monitoring for approximately 3 weeks is necessary. Continuous monitoring with devices from other manufacturers is limited to a few days due to concern that the emitted light can result in

low-temperature burns. However there is no such concern with the TOS-96, and long-term monitoring over many days can be performed.

#### **8) Testing and evaluation of peripheral and cerebral blood flow in outpatient neurosurgery, neurological checkups, and other areas of examination**

Examinations to evaluate surgery, circulatory status, and peripheral circulatory status:

The TOS-96 permits detection and evaluation of cerebral circulatory abnormalities, such as abnormal vascular reactivity and carotid artery stenosis resulting from balloon occlusion testing, temporary blockage of the internal carotid artery, the orthostatic test, and the hyperventilation test. It is used for evaluation of cerebral and peripheral blood flow and procedure selection in the angiography lab before aneurysmoplasty or carotid endarterectomy (CEA). A decrease in oxygen saturation would indicate that the test affected the region supplied by the blood vessel.

#### **9) Outpatient examination of cerebral blood flow in neurology and psychiatry**

Evaluation of drug efficacy and blood-flow reduction resulting from depression and vascular stenosis:

The patient's current condition and the effects of drug administration and treatment can be evaluated on an outpatient basis by performing rSO<sub>2</sub> testing and examining the patient's condition and values for rSO<sub>2</sub> and Hbl.

Patients with depression are thought to exhibit reduced blood flow in the frontal region. Thus, the TOS-96 can be used to examine higher-order brain function in psychiatric outpatient care.

\*Evaluation is possible by taking measurements before and after administration of a drug or other treatment, since in these cases blood flow increases in the frontal lobe regions used. The efficacy of a drug therapy can be evaluated based on symptomatic improvement and the increase in rSO<sub>2</sub> resulting from increased cerebral blood flow.

#### **10) Outpatient examination in vascular surgery**

Screening to ascertain whether gait disturbance is spinal or caused by intermittent claudication, evaluation of peripheral circulatory status, and evaluation of effects of surgery and the patient's postoperative condition:

With sensors attached to the calves of both legs, the patient is placed on a treadmill and the workload is gradually increased. rSO<sub>2</sub> is measured at the point where the patient complains of pain. If claudication is present, oxygen saturation is greatly reduced. However, with a spinal gait disturbance, pressure exerted on a nerve by the bone produces pain. In this case, there is no decrease in rSO<sub>2</sub>, permitting discrimination between gait disturbances resulting from claudication and those with a spinal cause.

The patient's status after lower extremity revascularization is evaluated by measuring the recovery time immediately following stress testing. If the postoperative recovery time is shorter than the preoperative time and there is a smaller rSO<sub>2</sub> decrease postoperatively, blood flow can be evaluated as having improved.

#### **11) Rehabilitation**

Evaluation of factors such as improvement in exercise capacity and skeletal muscle blood flow resulting from thermotherapy and various other treatments:

The TOS-96 can be used to evaluate muscle fatigue and metabolism under a load by measuring oxygen saturation in localized muscle tissue. Changes in motor function are associated with changes in blood flow in the muscles, and improvement in blood flow can be evaluated according to the increase in rSO<sub>2</sub>, while increases in blood flow are evaluated using Hbl. The TOS-96 sensor is waterproof, allowing sites that are immersed in water to be monitored.

\*Research on factors such as the relationship between blood flow and recovery of motor function is currently being conducted.